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**COMPUTER SUBROUTINES FOR THE ESTIMATION
OF NUCLEAR REACTION EFFECTS IN
PROTON-TISSUE-DOSE CALCULATIONS**

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COMPUTER SUBROUTINES FOR THE ESTIMATION OF NUCLEAR REACTION EFFECTS IN PROTON-TISSUE-DOSE CALCULATIONS

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SUMMARY

Calculational methods for estimation of dose from external proton exposure of arbitrary convex bodies are briefly reviewed and all the necessary information for the estimation of dose in soft tissue is presented. Special emphasis is placed on retaining the effects of nuclear reaction, especially in relation to the dose equivalent. Computer subroutines to evaluate all of the relevant functions are discussed. Nuclear reaction contributions for standard space radiations are in most cases found to be significant. Many of the existing computer programs for estimating dose in which nuclear reaction effects are neglected can be readily converted to include nuclear reaction effects by use of the subroutines described herein.

INTRODUCTION

When an object is exposed to external radiation, the dose field within the object is a complicated function of the character of the external radiation, the shape of the object (including orientation), and the object's material composition. Calculation of dose within an object involves solution of the appropriate Boltzmann transport equation in which the external radiation source imposes boundary conditions on the solution. Although general purpose computer programs exist for making such estimates (ref. 1), they are seldom used in practice when the object is bounded by a complicated surface, as is the human body, for example. Instead, calculations are usually made for simple geometric shapes from which inferences are then made for more general geometries, and the resultant errors are uncertain.

In the case of external proton radiation, such as that encountered near high-energy accelerators, in space, and in high-altitude aircraft, it is the inclusion of nuclear reaction effects which presents the major hurdles in an accurate calculation. It was found in reference 2 that dose estimation could be greatly simplified and still include the effects of nuclear reaction. Furthermore, it was shown that the method of reference 2, when in error, was always conservative. Required for such calculations is a knowledge of the

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transition of protons in semi-infinite slab geometry, which is the simplest geometry for existing transport computer programs. Indeed, almost everything that is known about the dose in humans from external proton radiation is inferred from calculations with slab geometry (ref. 3).

In the present report, a general method for estimation of dose in arbitrary convex geometry in terms of dose conversion factors in slab geometry is briefly discussed. These dose conversion factors for protons in tissue are then represented using buildup factors. A parametric form for the buildup factors is presented. The values for the parameters are derived from Monte Carlo calculations of various authors. All the information necessary to estimate dose and dose equivalent for proton irradiation of convex objects of arbitrary shape is contained herein. The advantage of the method is that existing proton dose calculations in which nuclear reactions are neglected can be directly converted by substitution of the dose conversion factors presented herein.

SYMBOLS

a_i	buildup-factor parameter, $i = 1, 2, 3, 4$
$D(\vec{x})$	dose at point \vec{x} , rad or rem
E	proton energy, MeV
E_0	proton energy parameter, MeV
E_r	reduced proton energy, MeV
$F(z, E)$	proton dose buildup factor, dimensionless
$P(E)$	nuclear survival probability in tissue
$p(E)$	particle rigidity, MV/c
p_0	particle rigidity parameter, MV/c
$Q_F(S)$	quality factor, dimensionless
$r(E)$	proton range in tissue

$R_n(z,E)$	dose conversion factor for normal incident protons, $\frac{\text{rad (or rem) cm}^2}{\text{proton}}$
$R_p(z,E)$	primary proton contribution to $R_n(z,E)$, $\frac{\text{rad (or rem) cm}^2}{\text{proton}}$
$R_s(z,E)$	secondary particle contribution to $R_n(z,E)$, $\frac{\text{rad (or rem) cm}^2}{\text{proton}}$
$S(E)$	proton energy loss rate in tissue, MeV/cm
\vec{x}	dose point position vector, cm
z	depth of penetration into a tissue slab, cm
$z_x(\vec{\Omega})$	distance from surface to dose point \vec{x} along direction $\vec{\Omega}$, cm
$\epsilon(z)$	energy of proton with range z in tissue, MeV
$\sigma(E)$	proton macroscopic cross section in tissue, cm^{-1}
$\tau(E)$	proton total optical thickness, dimensionless
$\phi(\vec{\Omega},E)$	proton differential fluence spectrum, $\text{protons/cm}^2\text{-MeV-sr}$
ϕ_0	proton differential fluence spectrum parameter, $\text{protons/cm}^2\text{-MeV-sr}$
$\vec{\Omega}$	unit vector in direction of proton motion, dimensionless

Abbreviations:

GCR	galactic cosmic radiation
SCR	solar cosmic radiation

A prime indicates a variable of integration.

THEORY

In passing through tissue, energetic protons interact mostly through ionization of atomic constituents by the transfer of small amounts of momentum to orbital electrons. Although the nuclear reactions are far less numerous, their effects are magnified because of the large momentum transferred to the nuclear particles and to the struck nucleus itself. Unlike the secondary electrons formed through atomic ionization by interaction with the primary protons, the resulting radiations of nuclear reaction are nearly all heavily ionizing and generally have large biological effectiveness. Many of the secondary particles of nuclear reactions are sufficiently energetic to promote similar nuclear reactions and thus cause a buildup of secondary radiations. The description of such processes requires solution of the transport equation. The approximate solution for the transition of protons in 30-cm-thick slabs of soft tissue for fixed incident energies are presented in references 4 to 11. The results of such calculations are dose conversion factors for relating the primary monoenergetic proton fluence to dose or dose equivalent as a function of position in a tissue slab.

Whenever the radiation is spatially uniform, the dose at any point \vec{x} in a convex object may be calculated according to reference 2 by

$$D(\vec{x}) = \int_0^\infty \int_{\Omega} R_n[z_x(\vec{\Omega}), E] \phi(\vec{\Omega}, E) d\vec{\Omega} dE \quad (1)$$

where $R_n(z, E)$ is the dose at depth z for normal incident protons of energy E on a tissue slab, $\phi(\vec{\Omega}, E)$ is a differential proton fluence along direction $\vec{\Omega}$, and $z_x(\vec{\Omega})$ is the distance from the boundary along $\vec{\Omega}$ to the point \vec{x} . It has been shown that equation (1) always overestimates the dose but gives an accurate estimate when the ratio of the proton beam divergence due to nuclear reaction to the body radius of curvature is small. Equation (1) is a practical prescription for introducing nuclear reaction effects into calculations of dose in geometrically complex objects such as the human body. The main requirement is that the dose conversion factors for a tissue slab be adequately known for a broad range of energies and depths.

Available information on conversion factors is for discrete energies from 100 MeV to 1 TeV in rather broad energy steps and for depths from 0 to 30 cm in semi-infinite slabs of tissue (refs. 4, 5, 8, and 9). The nuclear reaction data used for high-energy nucleons are usually based on Monte Carlo estimates (refs. 12 to 14) with low-energy neutron reaction data taken from experimental observation. The quality factor defined by the International Commission on Radiobiological Protection (ref. 15) is used for protons. The quality factor for heavier fragments and the recoiling nuclei is arbitrarily set to 20, which

is considered conservative, although the average quality factor obtained by calculation is comparable to estimates obtained through observations made in nuclear emulsion (ref. 16).

To fully utilize equation (1), the fluence-to-dose conversion factors for normal incident protons on a tissue slab must be known for all energies and depths. A parametrization of the conversion factors was introduced by Wilson and Khandelwal (ref. 2) which allowed reliable interpolation and extrapolation from known values. In the following section, a refinement and extension of that work will be discussed.

Fluence-to-Dose Conversion Factors

The conversion factor $R_n(z, E)$ is composed of two terms representing dose due to the primary beam protons and the dose due to secondary particles produced in nuclear reaction. Thus,

$$R_n(z, E) = R_p(z, E) + R_s(z, E) \quad (2)$$

where the primary dose equivalent conversion factor is given by

$$R_p(z, E) = P(E) Q_F[S(E_r)] \frac{S(E_r)}{P(E_r)} \quad (3)$$

The linear energy transfer (LET) denoted by $S(E)$ in equation (3) is calculated by using Bethe's formula above 243.8 keV as given by

$$S(E) = \frac{4\pi N_A e^4 z}{m_e v^2 A} \left\{ \ln \left[\frac{2m_e v^2}{I \left(1 - \frac{v^2}{c^2} \right)} \right] - \frac{v^2}{c^2} \right\} \quad (4a)$$

where

z	average tissue atomic number
A	average tissue atomic weight
I	adjusted ionization potential
m_e	electron mass
e	electron charge, C

v	proton velocity, cm/sec
c	velocity of light, cm/sec
N _A	Avogadro's number

At proton energies below 243.8 keV, the LET is calculated by the empirical expression

$$S(E) = E^{0.303}(2517 - 6283E) \quad (4b)$$

which approximately accounts for electron capture and the inner shell corrections in soft tissue. The proton range in soft tissue is given by

$$r(E) = \int_0^E \frac{dE'}{S(E')} \quad (5)$$

with the reduced energy in equation (3) given by

$$E_r = \epsilon[r(E) - z] \quad (6)$$

where $\epsilon(z)$ is the inverse function of $r(E)$. The total nuclear survival probability for a proton of energy E is given by

$$P(E) = \exp \left[- \int_0^E \sigma(E') \frac{dE'}{S(E')} \right] \quad (7)$$

where the macroscopic cross section $\sigma(E)$ for tissue as calculated by Bertini is given in reference 17. The proton total optical thickness given by

$$\tau(E) = \int_0^E \sigma(E') \frac{dE'}{S(E')} \quad (8)$$

is tabulated in table 1 for purposes of numerical interpolation. In the case of conversion factors for absorbed dose, $R_p(z, E)$ is taken as

$$R_p(z, E) = P(E) \frac{S(E_r)}{P(E_r)} \quad (9)$$

Buildup Factors

The representation of the conversion factors is simplified (see ref. 2) by rewriting equation (2) as

$$R_n(z, E) = \left[1 + \frac{R_s(z, E)}{R_p(z, E)} \right] R_p(z, E)$$

or

$$R_n(z, E) \equiv F(z, E) R_p(z, E) \quad (10)$$

where $F(z, E)$ is recognized as the proton dose buildup factor. The main advantage for introducing the buildup factor into equation (10) is that unlike $R_n(z, E)$, the buildup factor is a smoothly varying function of energy at all depths in the slab and can be approximated by the simple function

$$F(z, E) = (a_1 + a_2 z + a_3 z^2) \exp(-a_4 z) \quad (11)$$

where the parameters a_i are energy dependent. The a_i coefficients are found by fitting equation (11) to the values of the buildup factors as estimated from the Monte Carlo calculations of proton conversion factors. The resulting coefficients are shown in table 2. The coefficients for 100, 200, and 300 MeV protons were obtained by using the Monte Carlo data of reference 4. The values at 400, 730, 1500, and 3000 MeV were obtained from the results of Alsmiller, Armstrong, and Coleman (ref. 8). The 10 GeV entry was obtained from the calculations of Armstrong and Chandler (ref. 9). The values that are footnoted in table 2 were obtained by interpolating between data points or smoothly extrapolating to unit buildup factors at proton energies near the Coulomb barrier for tissue nuclei (≈ 12 MeV). The resulting buildup factors are shown in figures 1 and 2 and are compared with the Monte Carlo results; the error bars were determined by drawing smooth limiting curves to bracket the Monte Carlo values following the general functional dependence. These uncertainty limits should, therefore, be interpreted as limits of approximately two standard deviations, rather than the one standard deviation usually used in expressing uncertainty limits.

CONVERSION FACTOR COMPUTER CODE

To utilize equation (1) in a specific problem requires values for the conversion factor $R_n(z, E)$ over the range of interest. Formulas for these factors were presented in

the previous section. A computer code has been generated to return values of $R_n(z, E)$ for arbitrary depth z and energy E . This code is listed in the appendix and is described briefly here. There are six main functions to be generated relating to LET, range-energy relations, quality factor, and the functions relating to nuclear reaction effects given as nuclear survival probability and buildup factor.

The functions relating to ionization by the primary beam are generated by the function subroutine RTIS. Tables for $r(E)$ and $S(E)$ are generated on the first call to RTIS. Subsequent intermediate values are found by numerical interpolation above 10 KeV. A simplified approximation based on equation (4b) is used at lower energies. The function $\epsilon(z)$ is found by numerical inversion of $r(E)$.

The quality factor is approximated by

$$Q_F(S) \approx 0.06S^{0.8} \quad (12)$$

for S greater than 35 MeV/cm and set to unity for smaller LET.

The values shown in table 1 for the optical thickness are generated in the function subroutine PN and stored in an array for numerical interpolation; the nuclear survival probability is calculated using equation (7).

The coefficients for calculating the buildup factors are generated by subroutine ANTER as a function of energy by interpolating between the values shown in table 2.

The conversion factors are generated by subroutine RESP by supplying parameters z and E , which represent distance in centimeters of tissue and proton energy in mega-electron volts; respectively. The returned values of the conversion factors have units of rads (or rems) per proton per centimeter squared.

SAMPLE CALCULATIONS

To illustrate the usage of the buildup factors described here, calculations of the dose in slab geometry for normal incident protons with spectra typical of the space environment have been made; calculations were also made neglecting nuclear reaction effects. The percentage contribution to the absorbed dose and dose equivalent due to nuclear reactions are shown in figures 3 and 4, respectively. The spectra indicated by GCR in the figures represent galactic cosmic radiation with the spectrum given by

$$\phi_{\text{GCR}}(E) = \phi_0 \left(1 + \frac{E}{m_p}\right)^{-2.5} \quad (13)$$

The spectra denoted by the parameter p_0 represent solar cosmic ray spectra given as

$$\phi_{\text{SCR}}(E) = \phi_0 \exp\left[\frac{-p(E)}{p_0}\right] \quad (14)$$

with the rigidity given as

$$p(E) = \frac{1}{q} [E(E + 2m_p)]^{1/2} \quad (15)$$

where q is the proton charge and m_p is the proton mass. The value $p_0 = 100 \text{ MV/c}$ corresponds to an intermediate-energy solar event and $p_0 = 400 \text{ MV/c}$ corresponds to a high-energy solar event. The curve denoted by $E_0 = 100 \text{ MeV}$ represents the energetic inner belt protons with a spectrum

$$\phi(E) = \phi_0 \exp\left(\frac{-E}{E_0}\right) \quad (16)$$

It is clear from the figures that dose estimates for galactic cosmic rays and high-energy solar cosmic rays cannot be accurately calculated without proper account for nuclear reactions. This is especially true for estimates of the dose equivalent. Although reasonable estimates (± 10 percent) of low and intermediate solar cosmic ray absorbed doses are expected, the dose equivalent estimates must include nuclear reaction effects. Marginally good estimates of absorbed dose for inner belt protons can be made by neglecting nuclear reactions, but dose equivalent estimates require inclusion of nuclear reaction effects.

CONCLUDING REMARKS

A set of computer subroutines have been developed to estimate dose and dose equivalent in tissue for incident protons, and the use of these subroutines in dose calculations in complex geometry has been discussed. It was found that numerically the effects of nuclear reactions generally cannot be neglected in the calculation of doses due to space proton irradiation.

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May 3, 1976

APPENDIX

PROGRAM LISTING FOR CONVERSION FACTOR CALCULATION

The computer subroutines given in this appendix were developed for the present calculations, except for MGAUSS and IUNI which were taken from the mathematical subroutine library of the Langley Computer Complex.

APPENDIX

SUBROUTINE RESP(EN,X,RAD,REM)

C THIS SUBROUTINE GENERATES VALUES FOR THE SLAB CONVERSION FACTORS
C FOR VALUES OF PROTON ENERGY EN (MEV) AND DEPTH IN THE SLAB X (CM)

```

      REAL C(8)
      ENER=EN
      FX=X
      CALL ANTER(ENER,C,R)
      RRES=R-EX
      ENERP=ETIS(RRES)
      IF(ENERP)34.33.34
33    CONTINUE
      RAD=0.
      REM=0.
      RETURN
34    CONTINUE
      CALL APROB(EX,ENER,PROB)
      CALL ATOPP(ENERP,STOPP)
      CALL AF(STOPP,0.4LF)
2    PES=PROB*STOPP*0.4LF
22   PRINT 1,C
      COREQ=(C(1)+X*(C(2)+X*(C(3))))*EXP(-X*(C(4)))
      COREC=(C(5)+X*(C(6)+X*(C(7))))*EXP(-X*(C(8)))
      IF(COREQ.LT.1.) COREQ=1.
      IF(COREC.LT.1.) COREC=1.
      PRINT 1,EN,X,ENERP,PROB,STOPP,0.4LF,COREQ,COREC
1    FORMAT(2X,8F12.3)
      REM=PES*COREQ*1.6E-8
      PES=PROB*STOPP
      RAD=PES*COREC*1.6E-8
      RETURN
      END

```

SUBROUTINE ANTER(ENER,C,R)

C THIS SUBROUTINE GENERATES THE VALUES OF THE PARAMETERS
C OF THE ANALYTIC FITS OF THE MONTE CARLO RESULTS

```

      REAL C(8),A(12,8),E(12)
      LOGICAL FALS
      DATA E/30.,60.,100.,150.,200.,300.,400.,730.,1200.,1500.,3000.,
110000./
      DATA A/1.0,1.2,1.4,1.5,1.6,1.70,1.90,3.40,4.32,4.60,5.35,6.20,
2 0.0,0.0,0.02,0.07,0.09,0.11,0.13,0.156,0.167,0.170,0.190,0.280,
30.0,0.0,0.0,0.0,0.0,0.0,0.0,0.0,0.00035,0.00145,0.0025,0.0030,0.0035,
40.0,0.013,0.030,0.0385,0.040,0.033,0.0228,0.0150,0.013,0.012,0.010,0.010,
51.0,1.0,1.1,1.12,1.15,1.2,1.24,1.4,1.67,1.8,2.2,3.
60.0,0.01,0.040,0.05,0.052,0.068,0.071,0.09,0.094,0.095,0.10,0.11,
70.0,0.0,0.0,0.0,0.0,0.0,0.0,0.0,0.0001,0.00080,0.0015,0.002,0.00205,
80.0,0.01,0.026,0.031,0.032,0.026,0.0228,0.015,0.0122,0.012,0.01,0.01/
      DATA FALS/.T./
      DATA IPT/-1/
      R=RTIS(ENER)
      IF(FALS) GO TO 10
1    CONTINUE
      ELOG=ALOG(ENER)
      CALL IUNI(12,12,E,8,A,2,ELOG,C,IPT,IERR)
      RETURN
10   CONTINUE
      DO 11 I=1,12
      E(I)=ALOG(E(I))
11   CONTINUE
      FALS=.F.
      GO TO 1
      ENN

```

APPENDIX

SUBROUTINE AF(STOPP,QALF)

```

C   THIS SUBROUTINE COMPUTES THE QUALITY FACTOR AS A FUNCTION OF
C   LINEAR ENERGY TRANSFER
      IF(STOPP-35.)11,11,12
11  QALF=1.
      RETURN
12  QALF=.06*STOPP**.8
      RETURN
      END

```

SUBROUTINE APROB(EX,E,PROB)

```

C   THIS SUBROUTINE GENERATES VALUES FOR THE NUCLEAR SURVIVAL PROBABILITY
C   OF A PROTON OF ENERGY E (MEV) AFTER TRAVELING A DISTANCE EX (CM) IN TISSUE

      RRES=RTIS(E)-EX
      PROB=0.
      IF(RRES.LE.0.) RETURN
      ENEW=ETIS(RRES)
      PROB=PN(E)/PN(ENEW)
      RETURN
      END

```

FUNCTION PN(E)

```

C   PN GIVES PROBABILITY THAT PROTON TRAVELS FULL RANGE WITHOUT
C   BEING ABSORBED

      EXTERNAL FOX
      LOGICAL TRU
      REAL R(30),ET(30)
      DATA ET/0.,10.,25.,50.,100.,150.,200.,250.,300.,350.,400.,500.,
1700.,900.,1100.,1300.,1500.,1700.,2000.,2200.,2400.,2600.,2800.,
23000.,4000.,5000.,6000.,7000.,8500.,10000./
      DATA TRU/.T./
      DATA IPT/-1/
      IF(TRU) GO TO 10
111 ER=E
      CALL IUNI(30,30,ET,1,R,2,ER,BYRD,IPT,IERR)
      PN=EXP(-BYRD)
      RETURN
10  TRU=.F.
      R(1)=0.
      DO 1 I=2,30
        EU=ET(I)
        G=ET(I-1)
        CALL MGAUSS(G,EU,04,ANS,FOX,F,1)
        R(I)=R(I-1)+ANS
1  CONTINUE
      PRINT 19
19  FORMAT(///,25X,*PN GRID*//)
      PRINT 119
119 FORMAT (10X,*E VALUES FOR GRID*//)
      PRINT 226, ET
226 FORMAT (2X,8E15.6)
      PRINT 227
227 FORMAT (//,10X,*R VALUES FOR GRID*)
      PRINT 226,R
      GO TO 111
      END

```

APPENDIX

SUBROUTINE FOX(X,F)

```

ENER=X
3 CALL ASIGM(ENER,SIGMA)
  CALL ATOPP(ENER,STOPP)
  F=SIGMA/STOPP
2 RETURN
END

```

SUBROUTINE ASIGM(ENER,SIGMA)

C THIS SUBROUTINE GENERATES VALUES OF TOTAL NONELASTIC MACROSCOPIC
C CROSS SECTION (CM**2/G) IN TISSUE AS A FUNCTION OF PROTON ENERGY ENER(MEV)

```

REAL EN(43),CROSS(43)
DATA EN/25.32,29.86,34.16,39.86,44.65,50.01,60.19,70.24,79.47,89.9
11.100,8.117,9.139,3.156,3.175,3.186,6.202,7.266,1.304,7.375,2.407,
27.471,6.507,1.574,5.611,4.678,3.714,5.776,4.809,3.870,4.916,8.1007
3.,1129.,1406.,1796.,2024.,2318.,2071.,3408.,3943.,5000.,8000.,
41000./
DATA CROSS/2.614,2.360,2.153,1.985,1.887,1.757,1.621,1.526,1.451,1.
1379,1.327,1.261,1.211,1.187,1.164,1.152,1.141,1.097,1.087,1.100,1.
2136,1.199,1.212,1.266,1.293,1.350,1.379,1.424,1.440,1.471,1.478,1.
3504,1.477,1.480,1.483,1.485,1.487,1.475,1.461,1.463,1.46,1.458,
41.452/
DATA IPT/-1/
11 E=ENER
  IF(ENER.LT.25.32) ENER=25.32
  CALL IUNI(43,43,EN,1,CROSS,2,ENER,CROSS,IPT,IERR)
  SIGMA=(CROSS/100.)
  ENER=E
  RETURN
END

```

FUNCTION RTIS(E)

C THIS SUBROUTINE GENERATES THE RANGE-ENERGY RELATIONS AND LET FOR
C PROTONS IN TISSUE

```

EXTERNAL ATOF
REAL ET(57),RT(57),ST(57)
LOGICAL FALSE
DATA FALSE/.T./
DATA NP/57/
DATA ET/.01,.02,.03,.04,.05,.06,.07,.08,.09,.1,.2,.3,.4,.5,
1.6,.7,.8,.9,1.2,.3,.4,.5,.6,.7,.8,.9,10.,20.,30.,40.,50.,
260.,70.,80.,90.,100.,150.,200.,300.,400.,500.,600.,700.,
3800.,900.,1000.,1500.,2000.,2500.,3000.,4000.,5000.,6000.,
47000.,8500.,10000./
N=1
IF(FALSE) GO TO 10
12 CONTINUE
  RTIS=E**.697/(2517.*.697)
  IF(F.LT..01) RETURN
  A=ALOG(E)
  DO 1 IF=2,NP
    IF(A.LT.ET(IE)) GO TO 2
1 CONTINUE
2 I=IF
  SLOPE=(RT(I)-RT(I-1))/(ET(I)-ET(I-1))
  RAL=RT(I-1)+SLOPE*(A-ET(I-1))
  RTIS=EXP(RAL)
  RETURN
ENTRY STIS

```

APPENDIX

```

      N=2
      IF(FALSE)GO TO 10
13  CONTINUE
      RTIS=E**.303*(2517.-6283.*E)
      IF(E.LT..01) RETURN
      A=ALOG(E)
      DO 3 IE=2,NP
      IF(A.LT.ET(IE)) GO TO 4
3  CONTINUE
4  I=IE
      SLOPE=(ST(I)-ST(I-1))/(ET(I)-ET(I-1))
      SAL =ST(I-1)+SLOPE*(A-ET(I-1))
      RTIS=EXP(SAL)
      RETURN
      ENTRY ETIS
      N=3
      IF(FALSE)GO TO 10
14  CONTINUE
      RTIS=(2517.**.697*E)**1.43472
      IF(E.LT..01) RETURN
      R=ALOG(E)
      DO 5 IR=2,NP
      IF(R.LT.RT(IR)) GO TO 6
5  CONTINUE
6  I=IR
      SLOPE=(ET(I)-ET(I-1))/(RT(I)-RT(I-1))
      EAL =ET(I-1)+SLOPE*(R-RT(I-1))
      RTIS=EXP(EAL)
      RETURN
10  CONTINUE
      RT(1)=0.
      ST(1)=0.
      M=06
      DO 21 I=2,NP
      CALL ATOPP(ET(I),ST(I))
      CALL MGAUSS(ET(I-1),ET(I),M,ANS,ATOE,F,1)
21  RT(I)=RT(I-1)+ANS
      RIRST=RT(2)
      EIRST=ET(2)
      DO 11 IX=2,NP
      ET(IX)=ALOG(ET(IX))
      RT(IX)=ALOG(RT(IX))
11  ST(IX)=ALOG(ST(IX))
      FALSE=.F.
      GO TO (12,13,14)N
      END

```

SUBROUTINE ATOE(E,F)

```

      CALL ATOPP(E,S)
      F=1./S
      RETURN
      END

```

SUBROUTINE ATOPP(ENER,STOPP)

C THIS SUBROUTINE COMPUTES THE STOPPING POWER FOR PROTON IN TISSUE

```

      IF(ENER.GT..2438) GO TO 2
      STOPP=(2517.-6283.*ENER)*ENER**.303
      RETURN
2  ZETA=ENER/938.211
      BETAS=((ZETA*(ZETA+2.))/((ZETA+1.)**2))
      WBE=1.022201E6*BETAS/(1.-BETAS)
      FBET=ALOG(WBE)-BETAS
      STOPP=.30726148*(-2.2378342+.529726*FBET)/BETAS
      RETURN
      END

```


APPENDIX

SUBROUTINE MGAUSS(A,B,N,SUM,FUNC,FOFX,NUMBER)

```

    DIMENSION U(5),R(5),SUM(1),FOFX(1)
    DO 1 LL=1,NUMBER
1  SUM(LL)=0.0
    IF(A.EQ.B) RETURN
    U(1)=.425562830509184
    U(2)=.283302302935376
    U(3)=.160295215850488
    U(4)=.067468316655508
    U(5)=.013046735741414
    R(1)=.147762112357376
    R(2)=.13463335965499
    R(3)=.109543181257991
    R(4)=.074725674575290
    R(5)=.033335672154344
    FINE=N
    DELTA=FINE/(B-A)
    DO 2 K=1,N
    XI =K-1
    FINE=A+XI/DELTA
    DO 2 II=1,5
    UU=U(II)/DELTA+FINE
    CALL FUNC (UU,FOFX)
    DO 2 JOYBOY=1,NUMBER
2  SUM(JOYBOY)=R(II)*FOFX(JOYBOY)+SUM(JOYBOY)
    DO 3 JJ=1,5
    UU=(1.0-U(JJ))/DELTA+FINE
    CALL FUNC (UU,FOFX)
    DO 3 NN=1,NUMBER
3  SUM(NN)=R(JJ)*FOFX(NN)+SUM(NN)
    DO 7 IJK=1,NUMBER
7  SUM(IJK)=SUM(IJK)/DELTA
    RETURN
    END
    SUBROUTINE IUNI(NMAX,N,X,NTAB,Y,IORDER,X0,Y0,IPT,IERR)
C*****IUNI0010
C* IUNI0020
C* PURPOSE9 IUNI0030
C* SUBROUTINE IUNI USES FIRST OR SECOND ORDER IUNI0040
C* LAGRANGIAN INTERPOLATION TO ESTIMATE THE VALUES IUNI0050
C* OF A SET OF FUNCTIONS AT A POINT X0. IUNI IUNI0060
C* USES ONE INDEPENDENT VARIABLE TABLE AND A DEPENDENT IUNI0070
C* VARIABLE TABLE FOR EACH FUNCTION TO BE EVALUATED. IUNI0080
C* THE ROUTINE ACCEPTS THE INDEPENDENT VARIABLES SPACED IUNI0090
C* AT EQUAL OR UNEQUAL INTERVALS. EACH DEPENDENT IUNI0100
C* VARIABLE TABLE MUST CONTAIN FUNCTION VALUES CORRES- IUNI0110
C* PONDING TO EACH X(I) IN THE INDEPENDENT VARIABLE IUNI0120
C* TABLE. THE ESTIMATED VALUES ARE RETURNED IN THE Y0 IUNI0130
C* ARRAY WITH THE N-TH VALUE OF THE ARRAY HOLDING THE IUNI0140
C* VALUE OF THE N-TH FUNCTION VALUE EVALUATED AT X0. IUNI0150
C* IUNI0160
C* IUNI0170
C* USE9 IUNI0180
C* CALL IUNI(NMAX,N,X,NTAB,Y,IORDER,X0,Y0,IPT,IERR) IUNI0190
C* IUNI0200
C* PARAMETERS9 IUNI0210
C* IUNI0220
C* NMAX THE MAXIMUM NUMBER OF POINTS IN THE INDEPENDENT IUNI0230
C* VARIABLE ARRAY. IUNI0240
C* IUNI0250
C* N THE ACTUAL NUMBER OF POINTS IN THE INDEPENDENT IUNI0260
C* ARRAY,WHERE N.LE.NMAX. IUNI0270
C* IUNI0280
C* X A ONE-DIMENSIONAL ARRAY, DIMENSIONED (NMAX) IN THE IUNI0290
C* CALLING PROGRAM, WHICH CONTAINS THE INDEPENDENT IUNI0300
C* VARIABLES. THESE VALUES MUST BE STRICTLY MONOTONIC. IUNI0310
C* IUNI0320
C* NTAB THE NUMBER OF DEPENDENT VARIABLE TABLES IUNI0330
C* IUNI0340
C* Y A TWO-DIMENSIONAL ARRAY DIMENSIONED (NMAX,NTAB) IN IUNI0350
C* THE CALLING PROGRAM. EACH COLUMN OF THE ARRAY IUNI0360
C* CONTAINS A DEPENDENT VARIABLE TABLE IUNI0370
C* IUNI0380

```

APPENDIX

```

C*      IORDER      INTERPOLATION PARAMETER SUPPLIED BY THE USER.      *IUN10390
C*                                                         *IUN10400
C*      =0  ZERO ORDER INTERPOLATION9 THE FIRST FUNCTION      *IUN10410
C*      VALUE IN EACH DEPENDENT VARIABLE TABLE IS      *IUN10420
C*      ASSIGNED TO THE CORRESPONDING MEMBER OF THE Y0      *IUN10430
C*      ARRAY. THE FUNCTIONAL VALUE IS ESTIMATED TO      *IUN10440
C*      REMAIN CONSTANT AND EQUAL TO THE NEAREST KNOWN      *IUN10450
C*      FUNCTION VALUE.      *IUN10460
C*                                                         *IUN10470
C*      X0      THE INPUT POINT AT WHICH INTERPOLATION WILL BE      *IUN10480
C*      PERFORMED.      *IUN10490
C*                                                         *IUN10500
C*      Y0      A ONE-DIMENSIONAL ARRAY DIMENSIONED (NTAB) IN THE      *IUN10510
C*      CALLING PROGRAM. UPON RETURN THE ARRAY CONTAINS THE      *IUN10520
C*      ESTIMATED VALUE OF EACH FUNCTION AT X0.      *IUN10530
C*                                                         *IUN10540
C*      IPT      ON THE FIRST CALL IPT MUST BE INITIALIZED TO -1 SO      *IUN10550
C*      THAT MONOTONICITY WILL BE CHECKED. UPON LEAVING THE      *IUN10560
C*      ROUTINE IPT EQUALS THE VALUE OF THE INDEX OF THE X      *IUN10570
C*      VALUE PRECEDING X0 UNLESS EXTRAPOLATION WAS      *IUN10580
C*      PERFORMED. IN THAT CASE THE VALUE OF IPT IS      *IUN10590
C*      RETURNED AS9      *IUN10600
C*      =0  DENOTES X0 .LT. X(1) IF THE X ARRAY IS IN      *IUN10610
C*      INCREASING ORDER AND X(1) .GT. X0 IF THE X ARRAY      *IUN10620
C*      IS IN DECREASING ORDER.      *IUN10630
C*      =N  DENOTES X0 .GT. X(N) IF THE X ARRAY IS IN      *IUN10640
C*      INCREASING ORDER AND X0 .LT. X(N) IF THE X ARRAY      *IUN10650
C*      IS IN DECREASING ORDER.      *IUN10660
C*                                                         *IUN10670
C*      ON SUBSEQUENT CALLS, IPT IS USED AS A POINTER TO      *IUN10680
C*      BEGIN THE SEARCH FOR X0.      *IUN10690
C*                                                         *IUN10700
C*      IERR      ERROR PARAMETER GENERATED BY THE ROUTINE      *IUN10710
C*      =0  NORMAL RETURN      *IUN10720
C*      =J  THE J-TH ELEMENT OF THE X ARRAY IS OUT OF ORDER      *IUN10730
C*      =-1 ZERO ORDER INTERPOLATION PERFORMED BECAUSE      *IUN10740
C*      IORDER =0.      *IUN10750
C*      =-2 ZERO ORDER INTERPOLATION PERFORMED BECAUSE ONLY      *IUN10760
C*      ONE POINT WAS IN X ARRAY.      *IUN10770
C*      =-3. NO INTERPOLATION WAS PERFORMED BECAUSE      *IUN10780
C*      INSUFFICIENT POINTS WERE SUPPLIED FOR SECOND      *IUN10790
C*      ORDER INTERPOLATION.      *IUN10800
C*      =-4 EXTRAPOLATION WAS PERFORMED      *IUN10810
C*                                                         *IUN10820
C*      UPON RETURN THE PARAMETER IERR SHOULD BE TESTED IN      *IUN10830
C*      THE CALLING PROGRAM.      *IUN10840
C*                                                         *IUN10850
C*      REQUIRED ROUTINES      NONE      *IUN10860
C*                                                         *IUN10870
C*      SOURCE      CMPB ROUTINE MTLUP MODIFIED      *IUN10880
C*      BY COMPUTER SCIENCES CORPORATION*IUN10890
C*                                                         *IUN10900
C*      LANGUAGE      FORTRAN      *IUN10910
C*                                                         *IUN10920
C*                                                         *IUN10930
C*      DATE RELEASED      AUGUST 1,1973      *IUN10940
C*                                                         *IUN10950
C*      LATEST REVISION      JUNE 9, 1975      *IUN10960
C*                                                         *IUN10970
C*****IUN10980
C      DIMENSION X(1),Y(NMAX,1),Y0(1)      IUN10990
C      NM1=N-1      IUN11000
C      IERR=0      IUN11010
C      J=1      IUN11020
C      IUN11030
C      TEST FOR ZERO ORDER INTERPOLATION      IUN11040
C      IUN11050
C      DELX=X(2)-X(1)      IUN11060
C      IF (IORDER .EQ. 0) GO TO 10      IUN11070
C      IF (N.LT. 2) GO TO 20      IUN11080
C      GO TO 50      IUN11090

```

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10	IERR=-1	IUN11100
	GO TO 30	IUN11110
20	IERR=-2	IUN11120
30	DO 40 NT=1,NTAB	IUN11130
	Y0(NT)=Y(1,NT)	IUN11140
40	CONTINUE	IUN11150
	RETURN	IUN11160
50	IF (IPT .GT. -1) GO TO 65	IUN11170
C		IUN11180
C	CHECK FOR TABLE OF NODE POINTS BEING STRICTLY MONOTONIC	IUN11190
C	THE SIGN OF DELX SIGNIFIES WHETHER TABLE IS IN	IUN11200
C	INCREASING OR DECREASING ORDER.	IUN11210
C		IUN11220
	IF (DELX .EQ. 0) GO TO 190	IUN11230
	IF (N .EQ. 2) GO TO 65	IUN11240
C		IUN11250
C	CHECK FOR SIGN CONSISTENCY IN THE DIFFERENCES OF	IUN11260
C	SUBSEQUENT PAIRS	IUN11270
C		IUN11280
	DO 60 J=2,NM1	IUN11290
	IF (DELX * (X(J+1)-X(J))) 190,190,60	IUN11300
60	CONTINUE	IUN11310
C		IUN11320
C	IPT IS INITIALIZED TO BE WITHIN THE INTERVAL	IUN11330
C		IUN11340
65	IF (IPT .LT. 1) IPT=1	IUN11350
	IF (IPT .GT. NM1) IPT=NM1	IUN11360
	IN= SIGN (1.0,DELX * (X0-X(IPT)))	IUN11370
70	P= X(IPT) - X0	IUN11380
	IF (P* (X(IPT+1)- X0)) 90,180,80	IUN11390
80	IPT=IPT+IN	IUN11400
C		IUN11410
C	TEST TO SEE IF IT IS NECCESARY TO EXTRAPOLATE	IUN11420
C		IUN11430
	IF (IPT.GT.0 .AND. IPT .LT. N) GO TO 70	IUN11440
	IERR=-4	IUN11450
	IPT=IPT- IN	IUN11460
C		IUN11470
C	TEST FOR ORDER OF INTERPOLATION	IUN11480
C		IUN11490
C		IUN11500
90	IF (IORDER .GT. 1) GO TO 120	IUN11510
C		IUN11520
C	FIRST ORDER INTERPOLATION	IUN11530
C		IUN11540
	IPT1=IPT+1	IUN11550
	XTMP1=X0-X(IPT)	IUN11560
	XTMP2=X(IPT1)-X(IPT)	IUN11570
	XTMP1=XTMP1/XTMP2	IUN11580
	DO 100 NT=1,NTAB	IUN11590
	YTMP=Y(IPT1,NT)-Y(IPT,NT)	IUN11600
	YC(NT)=Y(IPT,NT)+YTMP*XTMP1	IUN11610
100	CONTINUE	IUN11620
	IF (IERR .EQ. -4) IPT=IPT+IN	IUN11630
	RETURN	IUN11640
C		IUN11650
C	SECOND ORDER INTERPOLATION	IUN11660
C		IUN11670
120	IF (N .EQ. 2) GO TO 200	IUN11680
C		IUN11690
C	CHOOSING A THIRD POINT SO AS TO MINIMIZE THE DISTANCE	IUN11700
C	BETWEEN THE THREE POINTS USED TO INTERPOLATE	IUN11710
C		IUN11720
	IF (IPT .EQ. NM1) GO TO 140	IUN11730
	IF (IPT .EQ. 1) GO TO 130	IUN11740
	A1=ABS(X0-X(IPT-1))	IUN11750
	A2=ABS(X(IPT+2)-X0)	IUN11760
	IF (A1-A2) 140,130,130	IUN11770
130	L=IPT	IUN11780
	GO TO 150	IUN11790
140	L=IPT -1	IUN11800
150	V1=X(L)-X0	IUN11810

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V2=X(L+1)-X0	IUNI1820
V3=X(L+2)-X0	IUNI1830
DO 160 NT=1,NTAB	IUNI1840
YY1=(Y(L,NT) * V2 - Y(L+1,NT) * V1)/(X(L+1) - X(L))	IUNI1850
YY2=(Y(L+1,NT)*V3-Y(L+2,NT) *V2)/(X(L+2)-X(L+1))	IUNI1860
Y0(NT)=(YY1*V3-YY2*V1)/(X(L+2)-X(L))	IUNI1870
160 CONTINUE	IUNI1880
IF (IERR .EQ. -4) IPT=IPT + 1N	IUNI1890
RETURN	IUNI1900
180 IF(P .NE. 0) IPT=IPT +1	IUNI1910
DO 185 NT=1,NTAB	IUNI1920
Y0(NT)=Y(IPT,NT)	IUNI1930
185 CONTINUE	IUNI1940
RETURN	IUNI1950
C	IUNI1960
C IERR IS SET TO THE SUBSCRIPT OF THE MEMBER OF THE TABLE	IUNI1970
C WHICH IS OUT OF ORDER	IUNI1980
C	IUNI1990
190 IERR=J +1	IUNI2000
RETURN	IUNI2010
200 IERR=-3	IUNI2020
RETURN	IUNI2030
END	IUNI2040

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TABLE 1. - TOTAL TISSUE OPTICAL THICKNESS
FOR PROTONS

E, GeV	$\tau(E)$	E, GeV	$\tau(E)$
0	0	1.3	6.57
.01	.0033	1.5	8.03
.025	.0171	1.7	9.52
.05	.0510	2.0	11.76
.1	.135	2.2	13.27
.15	.239	2.4	14.78
.2	.362	2.6	16.29
.25	.501	2.8	17.79
.3	.655	3.0	19.29
.35	.822	4.0	26.62
.4	1.004	5.0	33.81
.5	1.429	6.0	40.84
.7	2.471	7.0	47.75
.9	3.743	8.5	57.91
1.1	5.143	10.0	67.85

TABLE 2. - BUILDUP-FACTOR PARAMETERS

E, GeV	Buildup-factor parameters for dose equivalent				Buildup-factor parameters for absorbed dose			
	a ₁	a ₂	a ₃	a ₄	a ₁	a ₂	a ₃	a ₄
0.03	*1.00	*0	*0	*0	*1.00	*0	*0	*0
.06	*1.20	*0	*0	*.0130	*1.07	*.010	*0	*.010
.10	1.40	.020	0	.0300	1.10	.040	0	.026
.15	*1.50	*.070	*0	*.0385	*1.12	*.060	*0	*.031
.20	1.60	.090	0	.0400	1.15	.062	0	.032
.30	1.70	.110	0	.0330	1.20	.068	0	.026
.40	1.90	.130	0	.0228	1.24	.071	0	.0228
.73	3.40	.156	.00035	.0150	1.40	.090	.0001	.0150
1.2	*4.32	*.167	*.00145	*.0130	*1.67	*.094	*.0008	*.0122
1.5	4.60	.170	.00250	.0120	1.80	.095	.0015	.0120
3.0	5.35	.190	.00300	.0100	2.00	.100	.0020	.0100
10.0	6.20	.280	.00350	.0100	2.30	.111	.00205	.0100

*Values obtained by interpolation.

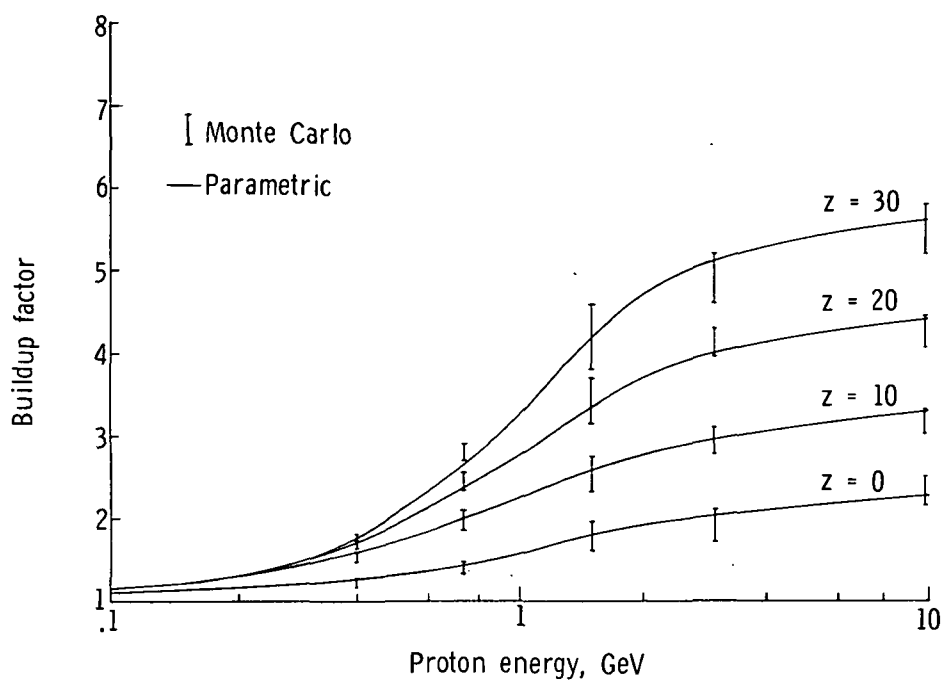


Figure 1.- Buildup factors for absorbed dose for several depths in tissue as a function of incident proton energy.

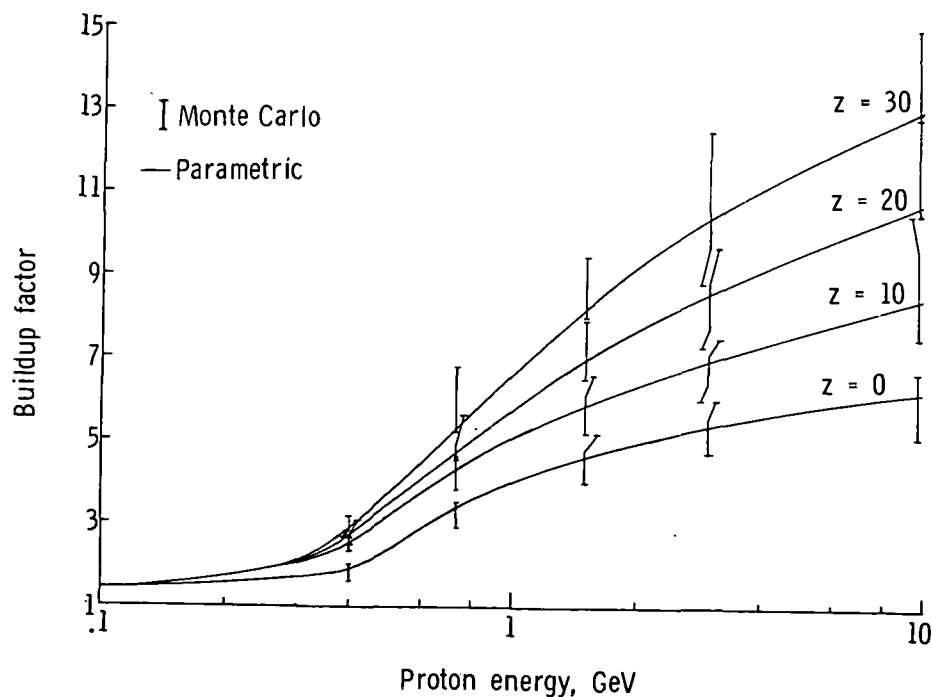


Figure 2.- Buildup factors for dose equivalent for several depths in tissue as a function of incident proton energy.

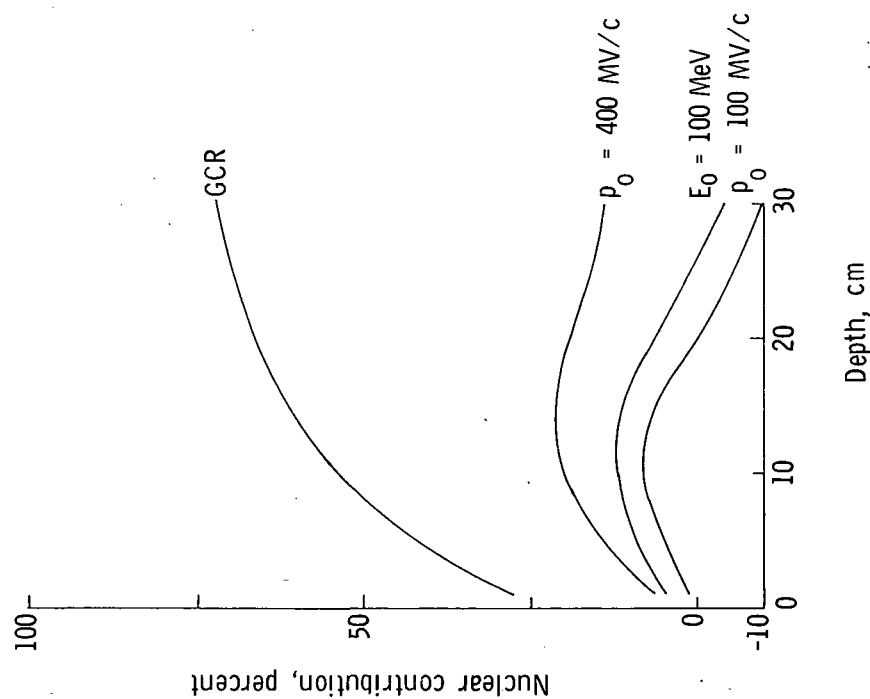


Figure 3.- Contribution of nuclear reactions to absorbed dose of the common space radiations.

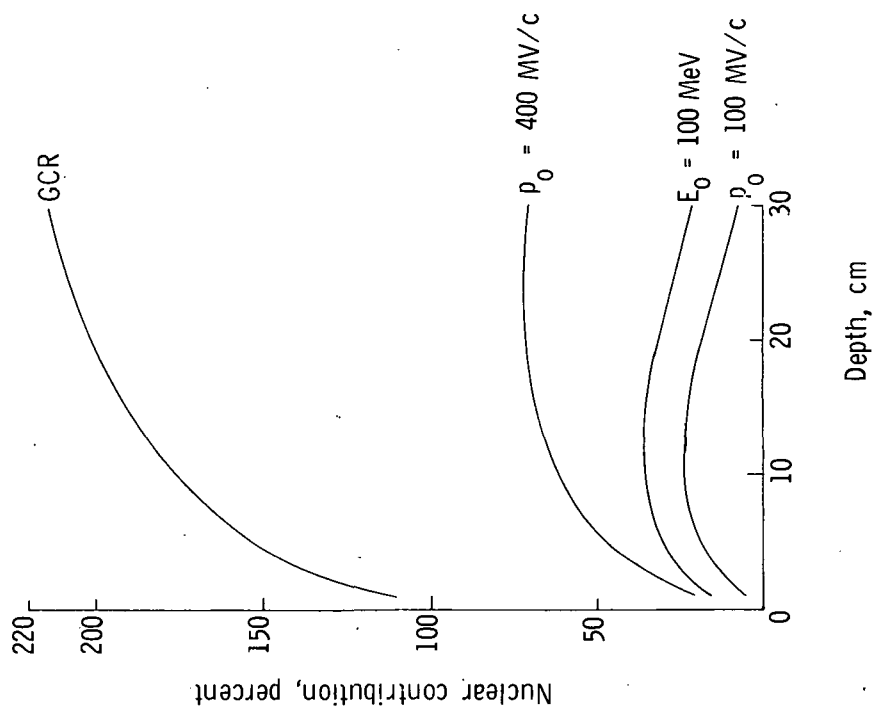


Figure 4.- Contribution of nuclear reactions to dose equivalent of common space radiations.



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